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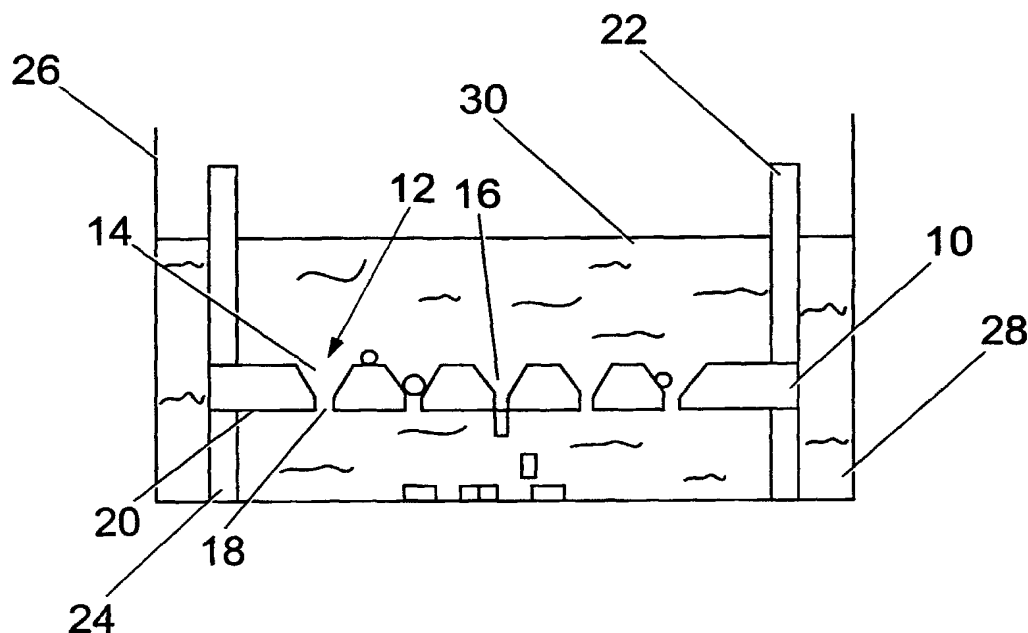
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[Continued on next page]

(54) Title: A CELL MIGRATION AND CHEMOTAXIS CHAMBER



(57) Abstract: The invention relates to a device for use in investigating and measuring migratory and invasive behaviour of cells and in the investigating of potential drugs and for clonal selection of cells from a mixed population. The device comprises a planar member such as a silicon wafer defining passageway(s) for cell movement where changes in physical parameters can be detected by means such as conductors.



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1   **"A Cell Migration and Chemotaxis Chamber"**

2

3   This invention relates to a cell migration and  
4   chemotaxis chamber for use in investigating and  
5   measuring the migratory and invasive behaviour of  
6   cells, and in the investigation of potential drugs, and  
7   to a method for producing such a chamber.

8

9   It is recognised that many of the most successful  
10   therapeutic drugs have, in the past, been found  
11   serendipitously. Given the millions of chemicals  
12   synthesised or extracted over the years it is expected  
13   that unsuspected potential drugs are to be found in  
14   this vast resource. To address this problem, many labs  
15   began to adopt a stochastic screening programme in  
16   which libraries of chemical compounds or natural  
17   products are tested for activity in robotic  
18   laboratories.

19

20   For example, the National Cancer Institute holds  
21   130,000 discrete extracts from plants, marine  
22   invertebrates and micro-organisms which it tests for  
23   effects on the growth of cancer cells or HIV (in its

1 anti-AIDS programme). However, apart from the  
2 important high through put screening methods for cell  
3 growth and cell death, the only other such screening  
4 methods available are dedicated to assaying drug  
5 effects on single oncogenes - for example the ability  
6 of a drug to bind to a cell surface receptor like the  
7 EGF receptor.

8

9 There is currently no automated screening method for  
10 cell migration nor for the invasive behaviour of cancer  
11 cells.

12

13 Assessment of the effects of potential drugs on cell  
14 migration is important in diseases where angiogenesis  
15 is involved. A second aspect of cell migratory  
16 behaviour, invasiveness, is important in cancer  
17 metastasis, where cancer cells migrate into and invade  
18 new tissue. Assessment of migratory behaviour is also  
19 important in basic research areas such as developmental  
20 biology, immunology and the like.

21

22 Angiogenesis is the formation of new blood vessels.  
23 Angiogenesis is utterly dependent upon the directional  
24 migration of endothelial cells towards the source of  
25 some angiogenic stimulating factor (chemotaxis). It is  
26 widely accepted that angiogenesis is an important  
27 target in a number of common diseases. For example,  
28 cancer metastasis, diabetic retinopathy, psoriasis and  
29 rheumatoid arthritis are all dependent on angiogenesis  
30 for their progression and could be treated by agents  
31 which inhibit angiogenesis. On the other hand, it  
32 would be desirable to screen for factors that promote

1 angiogenesis in the treatment of coronary artery and  
2 peripheral artery disease.

3

4 In vivo tests for angiogenic factors are expensive,  
5 time-consuming and provide few replicates (for example,  
6 the rabbit corneal pouch assay and the chick  
7 chorioallantoic membrane assay). Current in vitro  
8 screens for potential anti-angiogens are mostly  
9 dependent on measuring inhibition of cell migration  
10 towards an angiogenic stimulus such as cancer cell  
11 growth factors like EGF. However, these assays do not  
12 lend themselves to automation. Furthermore, even for  
13 manual basic research purposes the current assays are  
14 inefficient. Three main assays are in use:

15

16 1. The Boyden Chamber (and its modifications) consists  
17 of an upper chamber separated from a bottom chamber by  
18 a plastic membrane (typically polycarbonate) which has  
19 8  $\mu\text{m}$  pores in it. To assess chemotaxis, tissue culture  
20 medium containing chemoattractant is placed in the  
21 bottom chamber and medium containing cells is placed in  
22 the top chamber. The cells will then migrate towards  
23 the source of chemoattractant by squeezing through the  
24 pores (an animal cell is 20 $\mu\text{m}$  in diameter: cells cannot  
25 simply fall through the pores, but must use energy to  
26 locomote through). To measure chemoinvasion, the pores  
27 are first plugged with an extracellular matrix protein  
28 (like collagen). In this case, the cells must degrade  
29 the protein before they can pass through the pores.

30

31 1.2 Advantages

1 A large number of cells are monitored in each Boyden  
2 Chamber (1000-1 million), giving a more reliable  
3 estimate of drug effects. The assay does measure  
4 directional migration ("Chemotaxis"). Many replicates  
5 are possible, particularly when using inexpensive  
6 plastic disposable versions of the Boyden Chamber.

7

### 8 1.3 Problems

9 1.3a The main problem with the Boyden Chamber method is  
10 its quantification. Cells which migrate do not drop to  
11 the bottom of the chamber, but instead stick to and  
12 colonise the underside of the plastic membrane. In  
13 order to quantify migrated cells, the cells on the  
14 upper surface must first be carefully removed by  
15 scraping with a cotton bud. The membranes are delicate  
16 and easily punctured. The membrane is then stained  
17 with crystal violet (or some other cell stain) and the  
18 cells are either counted manually (using a microscope)  
19 or the cell-associated stain is re-dissolved and  
20 measured in a spectrophotometer. Manual cell counting  
21 is tedious and prone to operator error. Colorimetric  
22 assay of dye depends on there being sufficient numbers  
23 of invading cells (at least 1000) and is subject to  
24 interference because such dyes often bind to the  
25 proteins used to plug the pores, leading to  
26 unacceptably high background.

27

28 Cells will eventually fully colonise the underside of  
29 the membrane, and it is at this point that they start  
30 to drop off and fall to the bottom chamber where they  
31 can be stained and counted more easily. However, this  
32 typically takes a week, by which time a great deal of

1 cell division has occurred, particularly in the bottom  
2 chamber containing the growth factor. So, in this  
3 case, the number of cells in the bottom is a result of  
4 not just migration but also cell division.

5  
6 1.3b) A second problem with the Boyden Chamber is that  
7 it is a 'snap-shot'. That is, one knows how many cells  
8 migrate under treatment conditions compared with  
9 control but one has no idea of how fast the cells  
10 migrate. For example in a 48 hour migration assay both  
11 control and treatment membranes are fixed at 48 hours.  
12 All the cells might have migrated in the first 2 hours  
13 with no further movement in the following 46 hours, but  
14 the Boyden Chamber Assay will give no information on  
15 this.

16  
17 1.3c) The polycarbonate membrane fabrication process  
18 does not guarantee a fixed number of pores per chamber.

19  
20 1.3d) Re-usable Boyden Chambers are difficult to re-  
21 assemble - air bubbles often become trapped and it is  
22 easy to puncture new membranes. Disposable Boyden  
23 Chambers are similarly prone to membrane punctures.

24  
25 2) The Dunn Chamber  
26 The Dunn Chamber aims to address the problem of cell  
27 migration speeds. It consists of a specially  
28 constructed microspore slide with a central circular  
29 sink and a concentric annular moat. In this assay  
30 cells migrate on a coverslip (which is placed inverted  
31 on the Dunn Chamber) towards a chemotactic chemical.  
32 The cells are monitored over-night using a phase-

1 contrast microscope fitted with a video camera  
2 connected to a computer with image-grabber board. The  
3 microscope must have a heated stage and is usually  
4 fitted with an automatic electronic iris on its  
5 condenser.

6

## 7 2.1 Advantages

8 The Dunn Chamber measures directional migration  
9 continuously by means of time-lapse.

10

## 11 2.2) Problems

12 2.2a) A major problem with the Dunn Chamber Assay is  
13 that a very small number of cells are monitored  
14 (typically ten). This is a very small sample and  
15 average behaviour of this small sample may not  
16 therefore be typical of the population as a whole.

17

18 2.2b) A second major problem is that replication is  
19 very restricted. Each control chamber and each  
20 treatment chamber must be viewed in separate  
21 microscopes, each one similarly equipped with camera  
22 and computer. Each videomicroscopy unit would cost  
23 £20,000. So, to do three controls and three treatments  
24 would require an investment of £120,000, as experiments  
25 should ideally be performed on the same cell harvest  
26 and on the same day.

27

28 2.2c) Interpretation of the stored images requires  
29 bespoke software and a skilled operator. Present  
30 version of software requires manual logging of each  
31 cell's centre on each frame of the time-lapse video.  
32 This is highly time-consuming.



1 3. The Albrecht-Buhler Phagokinetic Track Assay  
2 An earlier cell motility/migration assay is, like the  
3 Dunn Chamber, dependent on measuring the tracks of  
4 cells. In this assay, coverslips are coated with  
5 colloidal gold particles. Cells are allowed to  
6 locomote over this gold lawn overnight. The cells  
7 clear tracks during their migration and the area of  
8 tracks gives an indication of the speed of motility.

9

10 3.1) Advantages

11 Many replicates are possible due to the cheapness of  
12 the assay. Only one microscope is required. Analysis  
13 is time-consuming unless automated image analysis is  
14 used. Although not monitored continuously, the cells  
15 leave a record of their overnight activity.

16

17 3.2) Problems

18 3.2a) The main problem with the Phagokinetic Track  
19 Assay is that it does not measure chemotaxis. Movement  
20 may be stimulated or inhibited, but the movement is  
21 random.

22

23 3.2b) A second major problem is that the cells ingest  
24 some of the gold particles. This is clearly not  
25 physiologically appropriate and it is unknown what  
26 effect this has on cells' behaviour or responses to  
27 added agents.

28

29 3.2c) A third difficulty with the assay is that the  
30 physical chemistry required to produce the gold colloid  
31 is difficult to replicate and scale-up. Differing

1 densities of gold coating and variation in particle  
2 size are encountered from batch to batch.

3

4 3.3d) Finally, cells often back-track, covering the  
5 same path more than once. So the observed track is not  
6 necessarily a true record of the cell's activity.

7

8 An object of the present invention is to solve or  
9 mitigate some of the above problems, particularly those  
10 relating to low numbers of replicates, expense and  
11 requirement for labour intensive and skilled  
12 interpretation and technical expertise.

13

14 According to the present invention there is provided a  
15 device for assessing cell migration, comprising a  
16 planar member presenting at least one passageway having  
17 a minimum dimension less than the cross-section of the  
18 cells of interest through which such cells can be  
19 caused to locomote, said passageway(s) being formed by  
20 etching a material which allows an aperture with a  
21 geometry which prevents adherence of the cells to the  
22 underside of the planar member.

23

24 Preferably, an array of passageways is provided,  
25 suitably a 10 x 10 array.

26

27 The planar member is preferably a silicon wafer, which  
28 may suitably be about 525 microns thick.

29

30 Said passageways are preferably etched to have the form  
31 of a hopper extending from a top surface and  
32 terminating in an aperture. Typically, the top of the

1   hopper will be a square of 700 microns per side, and  
2   the aperture will be a pore of about 8 microns per  
3   side.

4

5   Preferably, the device comprises the silicon wafer held  
6   between an upper cup into which a cell culture may be  
7   introduced, and a lower stand suitable for being  
8   received in a cluster plate well.

9

10   In one form of the invention, the silicon wafer is  
11   provided with means for sensing the passage of cells  
12   through the apertures. Said means may detect changes  
13   in a physical parameter, such as an electrical or  
14   optical criterion, as the cells pass. In one form,  
15   arrays of conductors are formed on the upper and lower  
16   surfaces of the wafers and disposed for sensing changes  
17   in an electrical parameter (such as resistance or  
18   capacitance) between conductors as cells pass through  
19   the apertures.

20

21   From another aspect, the present invention provides a  
22   method of making a planar member for use in a cell  
23   migration assessment device, the method comprising the  
24   steps of providing a planar member in the form of a  
25   wafer;

26

27         applying a resist pattern to an upper surface of  
28         the wafer to define an array of relatively large  
29         surface areas;

30

31         etching the upper surface for a time sufficient to  
32         expose the silicon in said array;

1       applying a resist pattern to a lower surface of  
2       the wafer to define a matching array of relatively  
3       small surface areas;  
4  
5       etching the lower surface for a time sufficient to  
6       expose the silicon in said surface areas; and  
7  
8       etching the exposed silicon at both surfaces to  
9       produce hopper-shaped openings from the top  
10      surface and connecting holes or pores through the  
11      bottom surface.  
12  
13     Typically, the wafer is of silicon, and the method is  
14     carried out using techniques known from processing of  
15     silicon integrated circuits.  
16  
17     The method may further comprise laying down a pattern  
18     of conductors on one or both surfaces for use in  
19     measuring an electrical parameter associated with each  
20     hole.  
21  
22     The invention further provides the use of a device as  
23     described herein for the selection of highly motile or  
24     invasive cells from a mixed population. This use can  
25     typically encompass clonal selection of cells.  
26  
27     Embodiments of the present invention will now be  
28     described, by way of example only, with reference to  
29     the drawings, in which:  
30  
31       Figure 1 is a perspective view of one form of  
32       chamber in accordance with the present invention;

1        Figure 2 illustrates the chamber of Figure 1 in  
2        use;

3  
4        Figure 3 is a schematic cross section  
5        corresponding to Figure 2;

6  
7        Figures 4a to 4e represents schematically stages  
8        in the production of part of the apparatus in  
9        Figures 1-3, and Fig. 5 is a schematic plan view  
10       illustrating a second embodiment; and

11  
12       Figure 5 is a schematic plan view illustrating a  
13       second embodiment.

14  
15       Referring to Figures 1-3, a cell migration and  
16       chemotaxis chamber consists of a silicon wafer 10 in  
17       which a 10mm X 10mm array of one hundred holes 12 have  
18       been etched. On the upper surface 14 the holes are  
19       700 $\mu$ m square cross-section leading, via a hollow  
20       inverted pyramidal 'hopper' 16, to a 8 $\mu$ m diameter exit  
21       pore 18 on the lower surface 20. The wafer 10 is  
22       sealed into a glass or plastic chamber, with an upper  
23       cup 22 and a lower stand 24. The chamber is designed  
24       to fit into standard disposable tissue culture cluster  
25       plates (12-well), and is used like a Boyden Chamber.  
26       The chamber is placed in a cluster plate well 26  
27       containing the medium plus chemoattractant 28 and the  
28       cells in control or drug-containing medium 30 is placed  
29       in the upper cup 22 above the silicon wafer 10. At the  
30       end of the experiment, the chamber is simply lifted out  
31       of the plate and the migrated cells (left behind in the

1 cluster plate well 26) are fixed, stained and cell-  
2 associated stain can be re-dissolved and read in a  
3 spectrophotometer.

4 The foregoing embodiment has the following advantages:

5

6 The cells do not stick to the lower surface 20 of the  
7 silicon wafer 10, but instead drop to the floor of the  
8 cluster plate well 26. This means that the upper  
9 surface 14 does not need to be scraped with a cotton  
10 bud (as is the case with the Boyden Chamber).

11

12 Since all the migrated cells are at the bottom of the  
13 cluster plate well 26, it is easy to fix and stain them  
14 allowing colorimetric assay of cell numbers.

15

16 Since the cells do not stick to the undersurface 20 of  
17 the wafer 10, non-specific staining of protein coatings  
18 does not interfere (as is the case with the Boyden  
19 Chamber).

20

21 Cells of interest will typically adhere to a plane  
22 silicon surface. It is believed that they do not  
23 adhere to the underside of the wafer 10 because of the  
24 hole geometry. The mechanism is not at present fully  
25 understood, but it is thought that the exit pore 18  
26 joining the lower face 20 in a relatively sharp edge is  
27 of significance.

28

29 A glass chamber of this embodiment can be re-used  
30 without difficult re-assembly (as is the case with the  
31 Boyden Chamber). To remove cells it is boiled in 5%  
32 tissue culture detergent then washed in distilled

1 water. It can then be re-sterilised by autoclave. If  
2 production were scaled up and wafers were encased in  
3 plastic chambers, they could be made cheap enough to be  
4 disposable.

5  
6 Each wafer 10 has exactly the same number of holes 12  
7 with very precise dimensions, making chemoattractant  
8 gradients between upper and lower wells more  
9 predictable and uniform (than is the case with the  
10 Boyden Chamber).

11  
12 The uniformity of numbers, and consistent geometry of  
13 the hoppers 16 and pores 18, would allow more  
14 consistent and reproducible protein coating or plugging  
15 of the wafer and/or pores 18.

16  
17 The consistent geometry of the array would allow for  
18 robotic dispensing of protein solutions into each  
19 hopper using a suitable array of micro-pipettes.

20  
21 Referring now to Figure 4 one example of a process for  
22 producing the silicon wafer of the foregoing embodiment  
23 will now be described.

24  
25 The starting material (Fig. 4A) was 4 inch diameter, n-  
26 type silicon wafers, <100> orientation, 9-16 ohm-cm  
27 resistivity, polished both sides and 525  $\mu\text{m}$  thick.

28  
29 The wafers were cleaned and coated with a 220 nm thick  
30 layer of LPCVD silicon nitride on all sides. Positive  
31 photoresist was deposited on the top side, prebaked and

1 exposed to UV light through an appropriately patterned  
2 chrome photo mask. The mask is aligned so that the  
3 edges of the square patterns lie along the 100  
4 directions. The exposed photoresist was developed to  
5 remove the resist from the square patterns. After  
6 baking the photoresist, the square patterns were  
7 reactive ion etched through the exposed silicon nitride  
8 on the top side. The photoresist was removed, and the  
9 wafers cleaned in a megasonic bath and then annealed at  
10 1000°C in N<sub>2</sub> for ten minutes (Fig. 4B).

11  
12 The bottom side of the wafer was coated with  
13 photoresist, which was pre-baked and exposed to UV  
14 light through a second patterned chrome photo mask.  
15 This second mask was aligned to the pattern on the  
16 other side of the wafer using an Electronic Visions  
17 EV420 double side mask aligner. The pattern was  
18 reactive ion etched through the nitride to expose the  
19 silicon (Fig. 4C).

20  
21 The silicon was anisotropically etched in a ternary  
22 mixture of KOH (50gm), IPA (51 cc) and DI-H<sub>2</sub>O (162 cc)  
23 at 80 ± 1°C in a lufran super bowl reflux system. This  
24 etch attacks the <100> planes at a much faster rate  
25 than the <111> planes to produce inverted square  
26 pyramid-like wells. The etching which took place from  
27 both sides was stopped once the wells from the two  
28 sides had met (Fig. 4D). This took about 5 hours. The  
29 silicon nitride layer was removed by wet chemistry and  
30 the wafer oxidised at 1050°C for one hour to grow a  
31 surface silicon dioxide layer of 100 nm (Fig. 4E). The



1 silicon wafer was then diced into 10mm square die to  
2 produce a number of Chambers.

3 A second type of a chamber in accordance with the  
4 invention will now be described.

5

6 This is designed to allow remote and continuous  
7 monitoring of cell migration with time. Emergence of a  
8 cell though each pore might be monitored in several  
9 different ways. Optical methods might be possible, but  
10 since cells are transparent it is likely that the cells  
11 would have to be dyed or fluorescently labelled which  
12 would be non-physiological. It is likely that  
13 electrical methods would be the most economical way to  
14 do this. For example changes in electrical resistance  
15 or capacitance would be sensed as a cell blocked the  
16 pore.

17

18 Based on this idea, the chamber of a further embodiment  
19 (Fig. 5) consists of a silicon chip resembling the  
20 first embodiment. In Figure 5, parts similar to those  
21 of the first embodiment are denoted by the same  
22 reference numerals. In this embodiment, however, upper  
23 and lower sets of conductors 50 and 52 are deposited on  
24 the surfaces 14 and 20 to allow detection of cells as  
25 they pass through each of the lower 8  $\mu\text{m}$  exit holes 18.  
26 Detection may be most easily achieved by measuring the  
27 change in electrical resistance as the cell blocks the  
28 hole 18 separating adjacent ones of the upper and lower  
29 conductors 50, 52. This could be detected as a  
30 resistance to the flow of electrical current between  
31 top and bottom conductors. The current would not be

1 continuous, but only applied momentarily when the array  
2 is being 'interrogated'. The array would be repeatedly  
3 scanned so that data is logged, with time, for each  
4 individual hole.

5

6 This arrangement means that cell migration can be  
7 monitored automatically and continuously during the  
8 experiment, rather than providing a mere 'snap-shot'

9

10 Cells do not have to be stained, removing the need for  
11 calibration of each cell-line (various cell types take  
12 up varying amounts of dye per cells) and removing  
13 interference from staining of coating protein.

14

15 The remote sensing capability of this embodiment  
16 combined with the low costs of silicon chip  
17 manufacturing mean that this method could be used in  
18 robotic drug screening.

19

20 Modifications may be made to the embodiments within the  
21 scope of the present invention.

1     **CLAIMS**

2

3     1.    A device for assessing cell migration, comprising  
4           a planar member presenting at least one passageway  
5           having a minimum dimension less than the cross-  
6           section of the cells of interest through which  
7           such cells can be caused to locomote, said  
8           passageway(s) being formed by etching a material  
9           which allows an aperture with a geometry which  
10          prevents adherence of the cells to the underside  
11          of the planar member.

12

13    2.    A device as claimed in claim 1 wherein an array of  
14          passageways is provided.

15

16    3.    A device as claimed in claim 1 or 2 wherein the  
17          planar member is a silicon wafer.

18

19    4.    A device as claimed in any of the preceding claims  
20          wherein said passageway(s) are etched to have the  
21          form of a hopper extending from a top surface and  
22          terminating in an aperture.

23

24    5.    A device as claimed in any preceding claims  
25          wherein the planar member is a silicon wafer and  
26          the silicon wafer is held between an upper cup  
27          into which a cell culture may be introduced, and a  
28          lower stand suitable for being received in a  
29          cluster plate well.

30

31    6.    A device as claimed in any preceding claim wherein  
32          the silicon wafer is provided with means for

1 sensing the passage of cells through the apertures  
2 wherein said means detect changes in a physical  
3 parameter as the cells pass.

4

5 7. A device as claimed in claim 6 wherein arrays of  
6 conductors are formed on the upper and lower  
7 surfaces of the wafers and disposed for sensing  
8 changes in an electrical parameter between  
9 conductors as cells pass through the apertures.

10

11 8. A method of making a planar member for use in a  
12 cell migration assessment device, the method  
13 comprising the steps of providing a planar member  
14 in the form of a wafer;

15

16 applying a resist pattern to an upper surface of  
17 the wafer to define an array of relatively large  
18 surface areas;

19

20 etching the upper surface for a time sufficient to  
21 expose the silicon in said array;

22

23 applying a resist pattern to a lower surface of  
24 the wafer to define a matching array of relatively  
25 small surface areas;

26

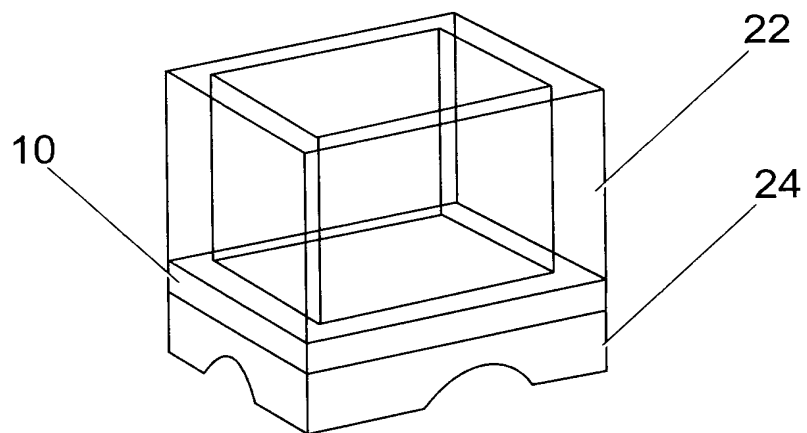
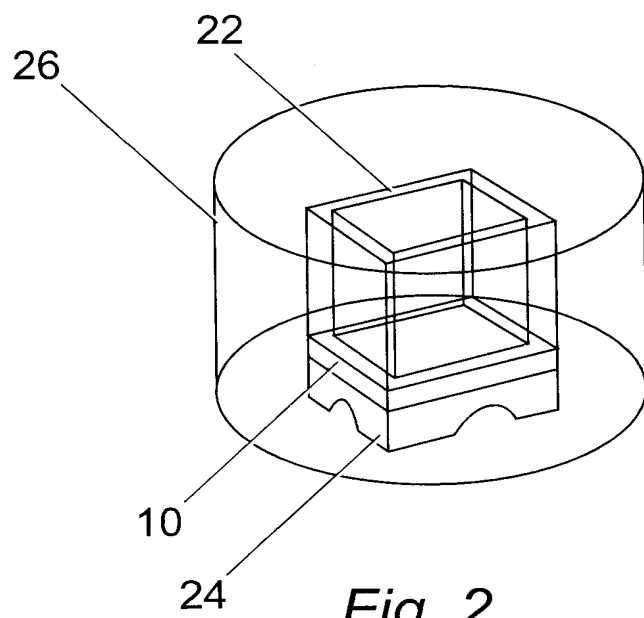
27 etching the lower surface for a time sufficient to  
28 expose the silicon in said surface areas; and

29

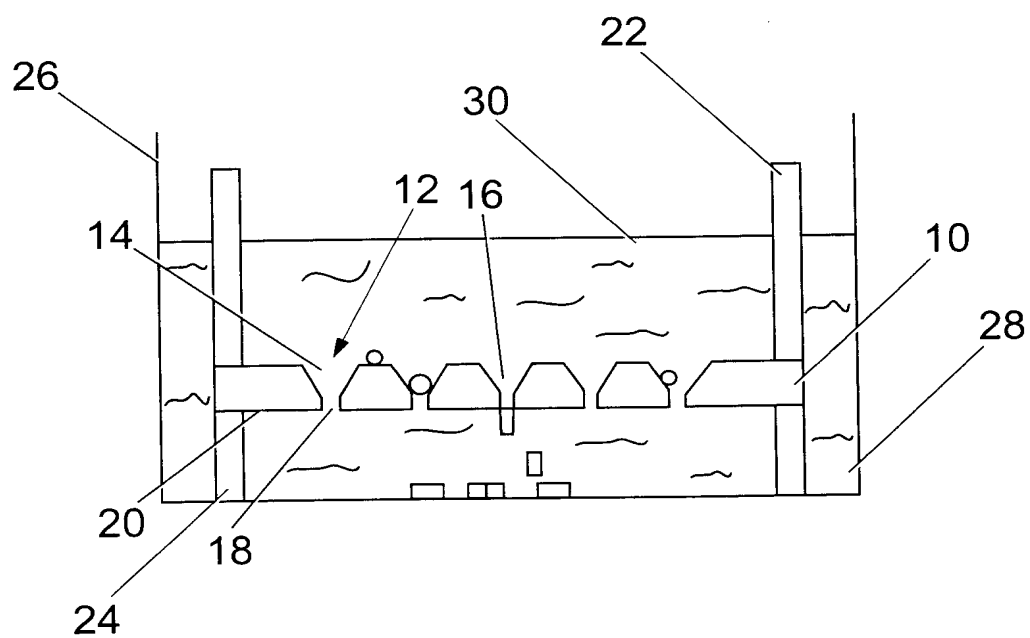
30 etching the exposed silicon at both surfaces to  
31 produce hopper-shaped openings from the top

- 1 surface and connecting holes or pores through the  
2 bottom surface.  
3
- 4 9. A method as claimed in claim 8 wherein the wafer  
5 is of silicon.  
6
- 7 10. A method as claimed in claim 8 or 9 wherein the  
8 method further comprises laying down a pattern of  
9 conductors on one or both surfaces for use in  
10 measuring an electrical parameter associated with  
11 each hole.  
12
- 13 11. Use of a device as claimed in any of claims 1 to 7  
14 for selection of highly motile or invasive cells.

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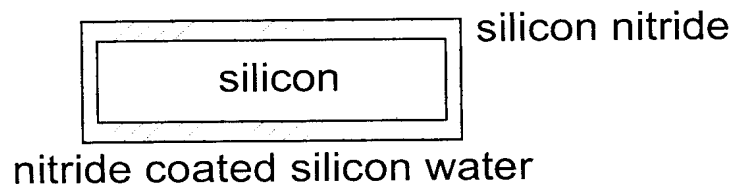
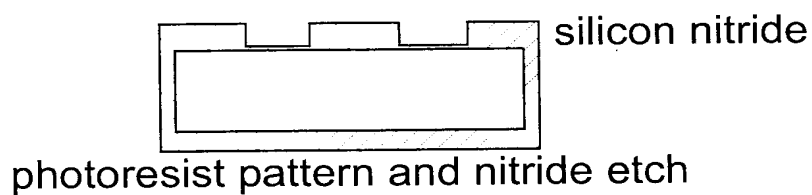
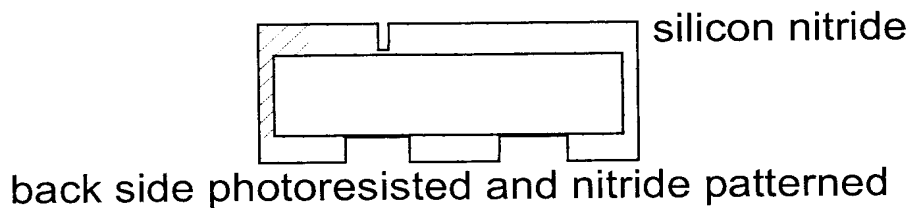
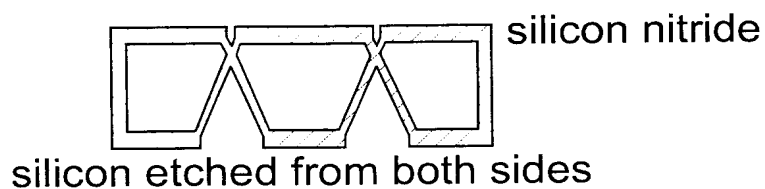
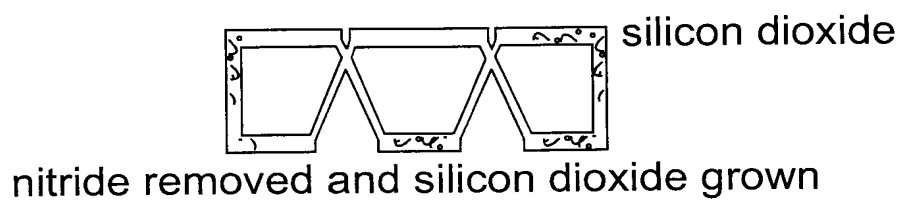


*Fig. 1*



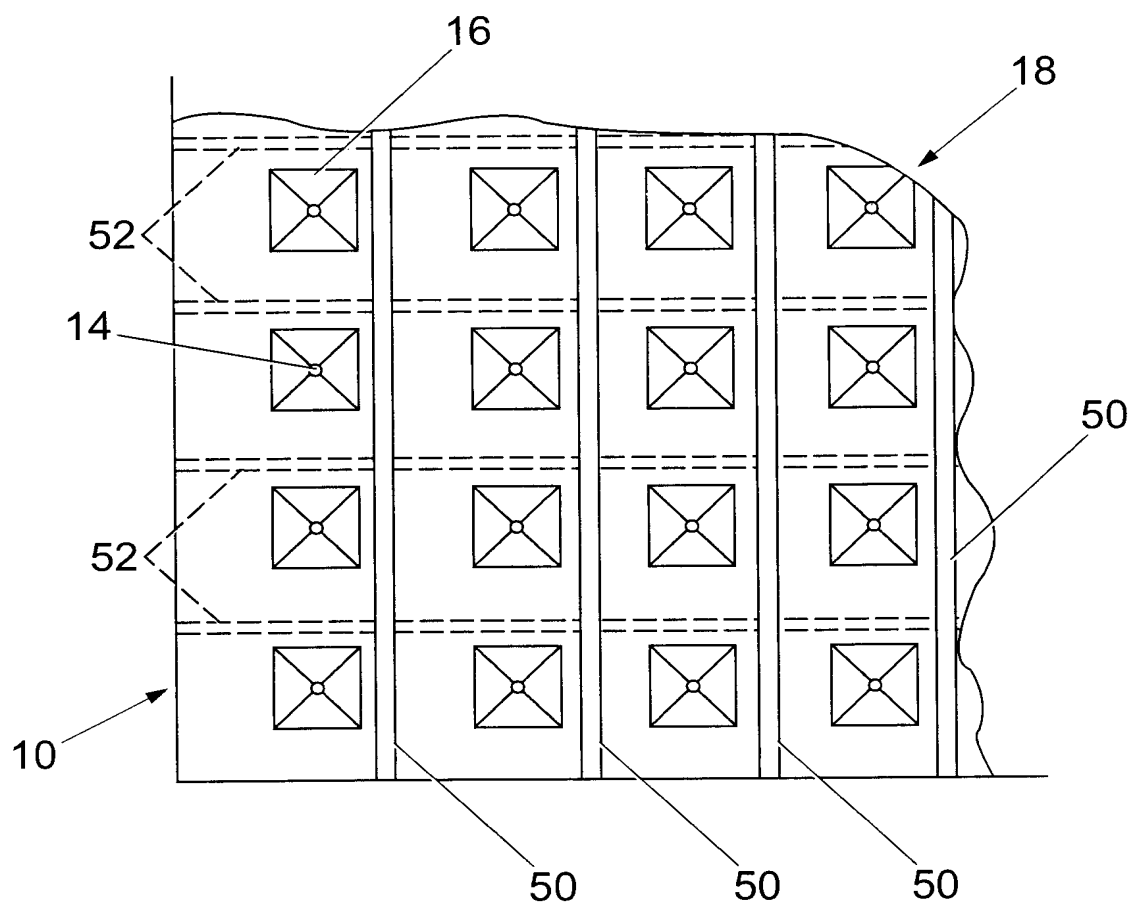
*Fig. 3*

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*Fig. 4A**Fig. 4B**Fig. 4C**Fig. 4D**Fig. 4E*



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*Fig. 5*

# INTERNATIONAL SEARCH REPORT

i. National Application No

PCT/GB 00/04213

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 7 C12M1/34 C12M3/04

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 C12M

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 729 949 A (DEUTSCH MORDECHAI ET AL) 8 March 1988 (1988-03-08) column 7, line 52; claims; figures column 24, line 47 - line 66 column 7, line 9 ---	1-11
X	US 4 895 805 A (SATO KAZUO ET AL) 23 January 1990 (1990-01-23) column 5, line 39 - line 48; claims; figures -----	1-6,8,9

☐

Further documents are listed in the continuation of box C.

☒

Patent family members are listed in annex.

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Date of the actual completion of the international search

28 February 2001

Date of mailing of the international search report

09/03/2001

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Coucke, A

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Information on patent family members

International Application No

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